



LOWER BODY NEGATIVE PRESSURE AS A SIMULATION METHOD FOR +GZ ACCELERATION STRESS: A FEASIBILITY AND COMPARATIVE ANALYSIS

Rafał LEWKOWICZ¹, Paulina BARAN², Mariusz KREJ², Mirosław DEREŃ², Łukasz DZIUDA²

¹ Simulator Study and Aeromedical Training Division, Military Institute of Aviation Medicine, Warsaw, Poland

² Department of Psychophysiological Measurements and Human Factor Research, Military Institute of Aviation Medicine, Warsaw, Poland

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Author's address: R. Lewkowicz, Military Institute of Aviation Medicine, Simulator Study and Aeromedical Training Division, Krasinskiego 54/56 Street, 01-755 Warsaw, Poland, e-mail: rlewkowicz@wiml.waw.pl

Introduction: This paper explores the utility of Lower Body Negative Pressure (LBNP) as a simulation method for replicating the physiological effects of +Gz acceleration stress experienced by aviators during high-performance flight maneuvers. The study investigates the feasibility of using LBNP to induce cardiovascular responses akin to those observed during +Gz acceleration, including changes in heart rate, blood pressure, stroke volume, cardiac output, mean arterial pressure, and central venous pressure.

Method: Through a comprehensive review of existing literature and empirical data (keywords and filters such as LBNP, aerospace, centrifuge, simulator, acceleration, Gz, and databases including PubMed, IEEE Xplore, ScienceDirect, and others relevant to this field of study were selected for the search), we evaluate the efficacy of LBNP in simulating the hemodynamic challenges associated with high-G environments.

Results: The results of the review were organized by thematic categories (advantages of the LBNP test compared to a human centrifuge, changes in heart rates during exposure to +Gz and in the LBNP test, and the relationship between tolerance to LBNP and G-tolerance level). Syntheses of the results are presented, highlighting key themes and insights.

Discussion and Conclusion: LBNP appears to be effective in simulating the impact of +Gz acceleration, particularly in conditions where the acceleration changes slowly (0.01 G/s) or moderately (0.05 G/s). Our findings suggest that LBNP holds promise as a versatile and practical tool for investigating physiological responses to +Gz acceleration stress and for advancing our understanding of human adaptation to extreme gravitational forces. Considering the high cost of installing a human centrifuge to assess +Gz acceleration tolerance, LBNP may serve as a cost-effective alternative for studying human physiology during exposure to moderate and slowly varying acceleration (+Gz).

Keywords: aviation medicine, LBNP, negative pressure, acceleration stress, centrifuge

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INTRODUCTION

Simulating G-forces acting on fighter pilots during flight maneuvers presents unique challenges on the ground. However, several methods can effectively simulate G-forces on the ground for training and research purposes. The most popular is the human training centrifuge simulator [51,65], designed for testing military pilot candidates and training pilots of highly maneuverable aircraft (i.e., combat, aerobatic, and sport), as well as for experimental technical testing. Moreover, the centrifuge provides a safe alternative for raising awareness among aircrews about the potential of adverse effects of acceleration, such as G-induced loss of consciousness (G-LOC) or spatial disorientation. This flight simulator is capable of reproducing a real flight [40,41,49,56,57], thereby ensuring the perfect professional preparation of pilots for complicated and dangerous air missions.

The Vertical Motion Simulator is another simulator for generating and studying the effects of G-forces on pilots during flight [4,5]. It consists of a platform capable of moving up and down along a vertical axis. By rapidly raising and lowering the platform, pilots can experience sensations similar to those of vertical acceleration. While not a perfect simulation of G-forces, this method can help familiarize pilots with the feeling of acceleration and deceleration.

Another example is the tilt platform, which consists of a table or chair mounted on a tilting mechanism. This design allows the simulation of sensations corresponding to different levels of acceleration (ranging from 1 to -1 g) along various axes. However, the platform can only simulate G-forces within a limited range. The next method used to simulate G-forces on the ground is the g-seat system [77–79]. This system is equipped with pneumatic pressure modules that provide sustained g-cueing. Multiple airbags in the seat and harness expand and contract to apply localized and sustained pressure, simulating the G-forces experienced during turns or maneuvers in an aircraft [77].

An alternative method for simulating +Gz stress and evaluating orthostatic response is a chamber that generates negative pressure in a pilot's lower body [50,55,68,70,76]. While not directly simulating G-forces, reducing the ambient pressure inside the chamber (around a pilot's lower body) can induce physiological effects similar to those experienced during high-G maneuvers, such as reduced blood flow to the brain, tachycardia, hypotension, and eventual loss of consciousness (i.e., presyncopal symptoms) [11,66,67,69].

A final example of a method for simulating the effects of G-forces on pilots during flight is virtual reality simulation [26,33]. This type of simulation can create immersive environments that replicate the visual and auditory aspects of flight maneuvers, including G-forces. While virtual reality alone cannot replicate the physical sensations of G-forces, it can be combined with motion platforms or other simulation techniques to enhance realism. Each of the methods mentioned above for simulating G-forces on the ground has unique advantages and challenges. The choice of method depends on factors such as the desired level of realism, available resources, and specific training objectives.

In this paper, we focused on the method by which the effects of G-forces are simulated using Lower Body Negative Pressure (LBNP). LBNP is a technique used to simulate the effects of gravity on the human body [42]. It involves creating a negative pressure (i.e., pressure below atmospheric level) around the lower limbs to induce cardiovascular and physiological responses similar to those under conditions of upright posture and gravitational stress [61,75].

LBNP was first used in research settings to study the effects of simulated gravitational changes on the human body, particularly in the field of aerospace medicine [7]. In space, astronauts experience microgravity, which can lead to physiological changes such as fluid redistribution, muscle atrophy, and cardiovascular deconditioning. By applying negative pressure to the lower body, LBNP effectively pulls blood towards the lower extremities, mimicking the gravitational forces that act on the human body when sitting or standing upright on Earth [19,20,45,46,48]. Researchers also use LBNP to simulate the effects of experiencing gravitational forces encountered during launch, re-entry, or planetary exploration [6,34,39,55]. This simulation enables the investigation of cardiovascular responses to changes in gravity and helps researchers develop countermeasures to mitigate the negative effects of space travel on astronaut health. Since its initial use in aerospace medicine research, LBNP has also found applications in other fields, such as orthostatic intolerance research [1,13,14,21,59–61], cardiovascular physiology studies [16,32,35,37,54,63], cerebral blood flow studies [18], and the development of medical interventions for conditions such as orthostatic hypotension and syncope [8,27,36,44].

Table 1. Result of the literature review.

Keyword	Phrase	Number of articles found in the database		
		PubMed	IEEE Xplore	ScienceDirect
LBNP	centrifuge	42	2	124
	aerospace	190	6	96
	simulator	403	1	22
	acceleration	78	2	142
	Gz	49	5	43

METHODS

The systematic literature review was based on searching, reviewing, and selecting articles based on predefined criteria. The selected databases were PubMed, IEEE Xplore, ScienceDirect. Searches were performed using predefined keywords (LBNP, aerospace, acceleration, centrifuge, simulator, and Gz). The search was not limited by publication date, language, or type of study. Table 1 presents the outcomes of the search conducted across the three databases, in accordance with the previously outlined criteria. A total of 71 articles were deemed eligible for analysis.

Advantages of LBNP over a human centrifuge

As an equivalent of the human centrifuge in terms of assessing acceleration tolerance in pilots (i.e., the pilot's ability to withstand high G-forces without losing consciousness) [3,25,74], LBNP offers several advantages [23]:

- allows the use of measurement techniques and technologies that are sensitive to movement or require a supine or sitting position (e.g., magnetic resonance imaging),
- keeps subjects in an unchanged position, enabling more efficient physiological measurements and avoiding the adverse effects of changing body position on the quality of signal recording, as observed in echocardiography and impedance reography; Nevertheless, for the low accelerations generated in the human centrifuge, when the test subject is not performing muscle tension maneuvers (no muscle contraction), physiological signals of good quality can also be obtained,
- enables the maintenance of central hypovolemia in the supine or sitting position, minimizing the influence of skeletal muscle activity. This allows for the study of isolated cardiovascular mechanisms involved in blood pressure control without considering the effects of the so-called muscle pump,
- ensures that the subject's head position remains unchanged, resulting in no stimulation

of the vestibular receptors. It is well-established that changes in head position can affect autonomic responses involved in blood pressure regulation [9]. When testing in a human centrifuge, both linear and angular accelerations are used to stimulate the vestibular organs, inducing variable postural muscle contractions,

- allows for easy dosing of the stimulus and rapid restoration of atmospheric pressure in the chamber in case of symptoms of threatened cardiovascular collapse. This facilitates quicker interruption and termination of the test, reducing the incidence of syncope [17],
- provides an opportunity to determine the total capacity of the cardiovascular system to regulate blood pressure, as well as to assess the compensatory reserve during central hypovolemia by allowing investigators to induce pre-fainting states under controlled and relatively safe experimental conditions,
- assures a more effective and practical way to simulate the effects of gravity on the cardiovascular system than centrifugation [72],
- is less stressful [50].

It is worth noting that one of the significant shortcomings of human centrifuges is the rotational movement of the cabin, which is a side effect of the generated linear acceleration (Gz). This movement causes strong stimulation of the semicircular canals of the vestibular system, known as the cross-coupling effect. Considering the relationship between vestibular organ excitation and autonomic responses in blood pressure regulation [9], as well as the potential for variable postural muscle contractions, the hemodynamic responses obtained in the human centrifuge may differ from those experienced during real flight. Therefore, it may be questionable whether the evaluation of LBNP-induced changes should be based on the cardiovascular response observed during the human centrifuge test or actual flight. The answer to this question can be found in studies that compare the differences in cardiovascular response between these two environments.

Table 2. Effect of +Gz acceleration and LBNP on selected hemodynamic parameters [24,55,64,67].

Parameter	Change under stimulus (↑ - increase, ↓ - decrease)	
	+Gz	LBNP (mmHg) *
Heart rate (HR)	↑	↑
Stroke volume (SV)	↑	↓
Cardiac output (CO)	↑	↓
Systolic/Diastolic blood pressure (SBP/DBP)	↑	↓
Mean arterial pressure (MAP)	↑	↓
Central venous pressure (CVP)	↑	↓

* LBNP-induced effects depend on the profile of changes (negative pressure value, duration, etc.) [24].

Despite the above-mentioned advantages of the LBNP in Gz simulation applications, the human centrifuge still remains the most reliable device and an essential tool in the preparation of pilots who are exposed to high levels of acceleration (G-forces). Compared to other alternative techniques for simulating Gz acceleration, including LBNP, the human centrifuge:

- includes the use of flight suits, helmets, and other equipment. Familiarity with these items in high-G conditions ensures that trainees can use them effectively during actual operations,
- helps strengthen the muscles used to counteract the effects of G-forces, particularly those involved in the Anti-G Straining Maneuver (AGSM),
- allows individuals to build G-tolerance, enabling them to withstand higher G-forces for longer durations. This capability is crucial for maintaining performance during combat maneuvers or emergency procedures,
- enables trainees to become familiar with the symptoms of G-stress, such as tunnel vision or gray-out,
- simulates the exact conditions of high-G environments encountered in flight or space missions. This realistic training ensures that individuals are well prepared for the specific challenges they will face.

Therefore, the use of a human training centrifuge in preparing individuals for the challenges of high-G environments does not appear to be quickly replaced by other Gz simulation techniques.

Table 2 shows the hemodynamic changes induced by +Gz and LBNP. The HR parameter consistently changes direction in response to both stimuli, while the other parameters show opposite changes.

Change in heart rate during exposure to +Gz and in the LBNP test

The first reports on the use of LBNP to simulate cardiovascular analogous to those elicited by +Gz acceleration stimuli date back to studies conduct-

ed in the 1970s. One such study [38] demonstrated that exposure to LBNP at -50 mmHg in the supine position induces changes in HR comparable to those observed in response to +2 Gz acceleration. In the standing position, ground acceleration (+1 Gz) result in a displacement of 500 to 600 ml of blood to the lower limbs. Additionally, there is a shift of fluids from the intravascular to the interstitial space and a decrease in cardiac output analogous to that induced by -40 mmHg LBNP in the supine position [2,31,52,62,75]. The HR values at -40 mmHg in the supine position (73.7 ± 2.6) were found to correspond to the control values without LBNP in the sitting position (74.1 ± 1.9 bpm). However, no significant differences were observed. A significant difference in heart rate was observed at -70 mmHg in the supine position (102.5 ± 4.4 bpm) and at -40 mmHg in the standing position (103.1 ± 4.0 bpm) [55].

Polese et al. [55] noted, however, that LBNP and human centrifuge are different physiological stressors and therefore induce different hemodynamic changes. Their findings indicated that peak HR values during exposure to +3 Gz (145.8 ± 7.7 bpm) and +4 Gz (152.3 ± 6.5 bpm) significantly exceeded the HR levels recorded during LBNP in the supine and standing positions [55]. For +2 Gz acceleration (104.8 ± 5.5 bpm), HR values closely matched those observed at -40 mmHg in the standing position (103.1 ± 4.0 bpm) and at -70 mmHg in the supine position (102.5 ± 4.4 bpm). Table 3 presents the LBNP values for which studies demonstrated consistency between HR changes observed during exposure to Gz acceleration and those induced by LBNP.

Polese et al. [55] also demonstrated that, in a subject in the upright position exposed to -40 mmHg LBNP (Table 3), mean arterial pressure (MAP) (90.6 ± 2.6 mmHg) and diastolic blood pressure (DBP) (75.8 ± 2.0 mmHg) were similar to the peak values observed during exposure to +2 Gz acceleration (93.2 ± 4.5 mmHg and 80.7 ± 5.5 mmHg, respectively). In the same study, venous

Table 3. LBNP values for which studies have shown HR changes to be consistent with those occurring during exposure to +Gz acceleration.

Acceleration	Heart rate (bpm)			Number of subjects	Reference
	M±SD	LBNP	M±SD		
+1 Gz	data not available	-40 mmHg in supine position	data not available	7	[53]
+1 Gz and tilt at 70°	90	-50 mmHg in supine position	90	5	[52]
+2 Gz	74.1 ± 1,9	-40 mmHg in a sitting posture	73.7 ± 2,6	8	[55]
combined +1 Gz and -40 mmHg in upright position	103.1 ± 4.0	-70 mmHg in supine position	102.5 ± 4.4	8	[55]
+2 Gz	104.8 ± 5.5	-40 mmHg in upright position	103.1 ± 4.0	8	[55]
		-70 mmHg in supine position	102.5 ± 4.4	8	

M – mean; SD – standard deviation

Table 4. Correlation between the scores obtained for the +Gz and LBNP stimulus tolerance tests [47].

		Gz onset		
		fast (0.2 G/s)	medium (0.05 G/s)	slow (0.01 G/s)
LBNP	fast (2.0 mmHg/s)	0.40	0.54	0.52
	medium (0.3 mmHg/s)	-0.05	0.25	0.53
	slow (0.067 mmHg/s)	-0.23	0.07	0.32

pooling in the lower limbs induced by LBNP in the sitting position, as measured by impedance plethysmography, was 65% of that recorded during +3 Gz and +4 Gz, and 64% of that during +2 Gz. These findings provide evidence that LBNP exposure at -40 mmHg in the sitting position can serve as a static simulator of HR and MAP changes induced by a gradually increasing acceleration stimulus of +2 Gz [55]. It was also found that during seated LBNP, blood pooling in the legs was significantly lower compared to acceleration [55]. The researchers suggested that LBNP at -80 or -90 mmHg during flight could simulate +2 Gz HR effects in the presence of weightlessness.

In a study conducted by Ludwig et al. [47], the tolerance of subjects to two stressors, LBNP and +Gz, was compared. The study involved 17 participants who were subjected to centrifugation and LBNP in the sitting position. Three different Gz onset rates (the rate of change in acceleration) were employed: 0.01 G/s (slow), 0.05 G/s (medium) and 0.2 G/s (fast). The rates of negative pressure change were 0.067 mmHg/s (slow), 0.3 mmHg/s (medium) and 2.0 mmHg/s (fast), respectively. It is worth noting that the Gz onset rates used in the study are significantly lower than those encountered during actual fighter jet flights. The results of this study demonstrating the relationship between human responses to LBNP and +Gz acceleration are presented in Table 4.

This study showed that the fastest rate of LBNP change (2.0 mmHg/s) is most strongly correlated with tolerance to slow (0.01 G/s) and medium (0.05 G/s) +Gz onset, but not with fast (0.2 G/s) +Gz onset. A moderate correlation was also observed between the medium rate of LBNP change (0.3 mmHg/s) and the slow (0.01 G/s) +Gz onset. These findings suggest that LBNP may only be a useful method for assessing +Gz tolerance to a limited extent when lower body decompression occurs at a sufficiently rapid rate.

In addition to the mapping the effects of +Gz stress in the LBNP test, it is also important to establish the correlation between +Gz tolerance levels determined using a human centrifuge and those obtained using LBNP.

Relationship between tolerance to LBNP and G-tolerance level

According to some researchers [50,55,68,70,76], the LBNP test is considered equivalent to human centrifuge testing due to similarities in the displacement of body fluids into the lower body and associated hemodynamic responses. Furthermore, some studies [71] indicate that LBNP has already been used as a method for estimating G-tolerance with a 90% accuracy level.

In studies [58,70,76], the possibility of applying the LBNP test to assess acceleration (+Gz) tolerance among military pilots was discussed. During

the LBNP test (-50 mmHg), a difference in the low-frequency component of HR variability was found between groups with high (+6.7-8.0 Gz) and low (+4.8-6.1 Gz) acceleration tolerance [76]. This component was higher in the latter group. The study also revealed a statistically significant decrease in sympathetic nervous system activity among participants with high acceleration tolerance during LBNP exposure at -50 mmHg.

In another study [50], a moderate correlation ($r=0.6$) between +Gz tolerance ($+5.94 \pm 0.98$ Gz) and QZ values (the time between ventricular depolarization [beginning of the Q wave in ECG] and the local maximum of the first derivative in impedance cardiography) was found. The LBNP test involved pilot candidates ($n=14$) who were exposed to -40 mmHg for 3 minutes in the supine position. For both baseline and maximal HR during LBNP (75 ± 12 bpm and 81 ± 13 bpm, respectively) and during +Gz (121 ± 19 bpm and 172 ± 21 bpm, respectively), the canonical correlation of exposure was $r=0.72$ (the result was statistically not significant). The researchers also indicated that high HR values prior to the centrifuge test in pilot candidates may lead to values that reach HR termination criteria [73]. As a result, tolerance to high +Gz forces may remain unrecognized. The authors suggest that the LBNP test could be a useful tool in selecting pilot candidates, particularly those with high baseline HR values.

Vergheze & Prasad [70] compared the increase in heart rate observed in LBNP tests (-40 mmHg for 5 minutes, both in supine and sitting postures) with that reported by Lindberg et al. [43] during +Gz stress. It was observed that the physiological strain (estimated based on HR) induced by -40 mmHg in the seated position is comparable to the level induced by between +2 and +3 Gz.

The LBNP test for the pre-selection of pilots with low +Gz tolerance was also developed by Hanousek et al. [29]. The authors verified this method by comparing the physiological responses of pilots during LBNP, flight, and centrifuge load. The study found that changes in blood pressure and HR during the LBNP test were similar to those observed during exposure to +3.5 Gz in a human centrifuge [12]. The results also mostly corresponded to acceleration of +4.5 Gz during flight in a real aircraft [30]. In subsequent studies, Hanousek et al. [28] reconstructed the LBNP device not only to estimate the +Gz tolerance level but also to identify pilots with low tolerance to the push-pull effect.

In other studies [67,69] researchers examined the relationship between six parameters (arterial blood pressure, HR, thoracic impedance reogra-

phy, non-standard electrocardiographic leads, phonocardiography, and air plethysmography on the middle finger of the right hand) measured during a 20-minute-long LBNP and during +Gz tolerance tests. This analysis revealed, with high statistical significance ($p<0.01$), that based on responses to the LBNP test (six parameters mentioned above), it is possible to group subjects according to their +Gz tolerance. The accuracy of the decision making during this selection was 82.1%. A strong dependence of +Gz acceleration tolerance on six listed hemodynamic and hormonal parameters, measured during LBNP exposure at -60 mmHg for supine subjects ($n=65$), was described by the following linear equation [67]:

$$+GZ = -0.13PRA + 0.01LVET + 0.005CO + 0.01PEP + 0.11PAC + 0.01HR + 2.18 \quad (1)$$

where:

PRA – plasma renin activity,

LVET – left ventricular ejection time, calculated as the time between the beginning of the ascendant arm of the dZ/dt wave and the dicrotic notch on the same wave (dZ/dt) [msec],

CO – cardiac output, calculated as the product of stroke volume and heart rate [ml/min],

PEP – pre-ejection period, calculated as the time between the beginning of the QRS complex and the beginning of the ascendant arm of the dZ/dt wave (the first derivative of the reography wave dZ) [msec],

PAC – aldosterone,

HR – heart rate.

Equation (1) can be used to predict the individual +Gz tolerance values with a mean error of 0.26 G. Researchers using LBNP have noted that this test may lead to vasovagal syncope and/or cardiac arrhythmias. Therefore, caution should be exercised when performing LBNP tests, with appropriate monitoring of physiological parameters and the presence of medical personnel, such as a physician.

Finally, it should be noted that the definition of G-tolerance was not uniform across the reviewed studies. While some focused on autonomic nervous system responses (e.g., HR variability, HR changes), others relied on cardiac hemodynamics or multi-parametric models. These differences could influence comparability between studies, emphasizing the need for standardized criteria in future LBNP studies on G-tolerance assessment methods.

CONCLUSIONS

In summary, LBNP has the potential to simulate +Gz acceleration and generate reproducible physiological responses. However, before any ap-

plication, LBNP-based methods must be properly validated to ensure their effectiveness.

Considering the high cost of the installing a human centrifuge to assess +Gz acceleration tolerance, LBNP may serve as a cost-effective alternative for studying human physiology during exposure to moderate and slowly varying acceleration (+Gz) [15,22]. It is important to note, however, that

LBNP-induced hemodynamic and neurohormonal responses, as well as tolerance, vary among individuals [10,24]. Therefore, when designing experiments and selecting participants, it is important to consider the various factors (i.e., participant-specific and LBNP protocol-related variables) that may influence LBNP-induced responses.

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The authors declare that there is no conflict of interest.

REFERENCES

1. Arbeille P, Kerbeci P, Mattar L, Shoemaker JK, Hughson RL. Insufficient flow reduction during LBNP in both splanchnic and lower limb areas is associated with orthostatic intolerance after bedrest. *Am J Physiol Hear Circ Physiol. American Physiological Society*; 2008; 295(5):H1846–H1854.
2. Baisch FJ, Petrat G. Body fluid distribution in man in space and effect of lower body negative pressure treatment. *Clin Investig. Springer Science and Business Media LLC*; 1993; 71(9):690–9.
3. Barański S, Markiewicz L, Wojtkowiak M, Sokołowski E. The role of physical training in increasing +Gz tolerance in the initial phase of aviation training. *Physiologist*. 1988; 51:24–7.
4. Beard SD, Reardon SE, Tobias EL, Aponso BL, Beard AD, Reardon SE, et al. Simulation system fidelity assessment at the Vertical Motion Simulator. In: *American Helicopter Society (AHS) Annual Forum and Technology Display*. Phoenix, (AZ), US: American Helicopter Society International, Inc.; 2013. pp. 1–16.
5. Beard SD, Reardon S, Tobias EL, Aponso BL. Simulation System Optimization for Rotorcraft Research on the Vertical Motion Simulator. In: *AIAA Modeling and Simulation Technologies Conference*. Minneapolis, Minnesota: Ames Research Center; 2012.
6. Berry CA. Medical legacy of Apollo. *Aerosp Med. United States*; 1974; 45(9):1046–57.
7. Campbell MR, Charles JB. Historical review of lower body negative pressure research in space medicine. *Aerosp Med Hum Perform*. 2015; 86(7):633–40.
8. Convertino VA. Lower body negative pressure as a tool for research in aerospace physiology and military medicine. *J gravitational Physiol a J Int Soc Gravitational Physiol. United States*; 2001; 8(2):1–14.
9. Convertino VA. Mechanisms of blood pressure regulation that differ in men repeatedly exposed to high-G acceleration. *Am J Physiol Regul Integr Comp Physiol. American Physiological Society*; 2001; 280(4):R947–58.
10. Convertino VA, Ludwig DA, Cooke WH. Stroke volume and sympathetic responses to lower-body negative pressure reveal new insight into circulatory shock in humans. *Auton Neurosci Basic Clin*. 2004; 111(2):127–34.
11. Dikshit MB. Lower-body suction and cardiovascular reflexes: physiological and applied considerations. *Indian J Physiol Pharmacol. India*; 1990; 34(1):3–12.
12. Doseł P, Hanousek J, Cmiral J, Petricek J. Physiological response of pilots to the LBNP, flight and centrifuge load. *J gravitational Physiol a J Int Soc Gravitational Physiol*. 1998; 5:P41-2.
13. Dziuda Ł, Krej M, Śmietanowski M, Sobotnicki A, Sobiech M, Kwaśny P, et al. Development and evaluation of a novel system for inducing orthostatic challenge by tilt tests and lower body negative pressure. *Sci Rep*. 2018; 8(1):1–15.
14. El-Bedawi KM, Hainsworth R. Combined head-up tilt and lower body suction: A test of orthostatic tolerance. *Clin Auton Res. Springer Science and Business Media LLC*; 1994; 4(1-2):41–7.

15. Evans JM, Knapp CF, Goswami N. Artificial gravity as a countermeasure to the cardiovascular deconditioning of spaceflight: Gender perspectives. *Front Physiol.* 2018; 9:716.
16. Fortney SM, Tankersley C, Lightfoot JT, Drinkwater D, Clulow J, Gerstenblith G, et al. Cardiovascular responses to lower body negative pressure in trained and untrained older men. *J Appl Physiol (Bethesda, Md 1985).* 1992; 73(6):2693–700.
17. Gąsiorowska A. Hemodynamiczne i neurohormonalne reakcje na podciśnienie zastosowane na dolną połowę ciała u zdrowych mężczyzn: wpływ treningu i 3-dniowego pozostawania w pozycji leżącej. *Polska Akademia Nauk;* 2008.
18. Gazdziński SP, Kowalczyk K, Zieliński P, Baran P, Krej M, Dziuda Ł. Lower body negative pressure training leads to lasting reduction in cerebral blood flow: A preliminary study using arterial spin labeling perfusion MRI. *Polish J Aviat Med Bioeng Psychol. Military Institute of Aviation Medicine;* 2020; 24(4):36–46.
19. Gzenko OG, Genin AM, Egorov AD. Summary of medical investigations in the U.S.S.R manned space missions. *Acta Astronaut. Elsevier BV;* 1981; 8(9–10):907–17.
20. Gerber B, Singh JL, Zhang Y, Liou W. A computer simulation of short-term adaptations of cardiovascular hemodynamics in microgravity. *Comput Biol Med. Elsevier Ltd;* 2018; 102(July):86–94.
21. Gerega A, Wojtkiewicz S, Sawosz P, Kacprzak M, Toczyłowska B, Bejm K, et al. Assessment of the brain ischemia during orthostatic stress and lower body negative pressure in air force pilots by near-infrared spectroscopy. *Biomed Opt Express.* 2020; 11(2):1043–60.
22. Goswami N, Batzel J, Clément G, Stein TP, Hargens AR, Sharp MK, et al. Maximizing information from space data resources: a case for expanding integration across research disciplines. *Eur J Appl Physiol.* 2013; 113(7):1645–54.
23. Goswami N, Blaber AP, Hinghofer-Szalkay HG, Convertino VA. Lower body negative pressure: Physiological effects, applications, and implementation. *Physiol Rev.* 2019; 99(1):807–51.
24. Goswami N, Loeppky JA, Hinghofer-Szalkay HG. LBNP: Past protocols and technical considerations for experimental design. *Aviat Sp Environ Med.* 2008; 79(5):459–71.
25. Grönkvist M, Levin B, Eiken O. G tolerance during open- vs. Closed-loop G-time control. *Aerosp Med Hum Perform.* 2018; 89(9):798–804.
26. Gugenheimer J, Wolf D, Eiriksson ER, Maes P, Rukzio E. GyroVR: Simulating inertia in virtual reality using head worn flywheels. In: *UIST 2016 - Proceedings of the 29th Annual Symposium on User Interface Software and Technology.* Association for Computing Machinery, Inc; 2016. p. 227–32.
27. Hachiya T, Blaber AP, Saito M. Changes in superficial blood distribution in thigh muscle during LBNP assessed by NIRS. *Aviat Space Environ Med.* 2004; 75(2):118–22.
28. Hanousek J, Dosel P, Petricek J, Cettl L. Push-Pull Effect Simulation by the LBNP Device. *IFMBE Proc.* 2009; 23:1564–8.
29. Hanousek J, Dosel P, Petricek J, Cettl L. Blood pressure response to LBNP load in various types of examinations BT. In: *Vander Sloten J, Verdonck P, Nyssen M, Haueisen J, editors. 4th European Conference of the International Federation for Medical and Biological Engineering.* Berlin, Heidelberg: Springer Berlin Heidelberg; 2009. pp. 1552–5.
30. Hanousek J, Petricek J. Comparison of pilots' physiological responses to the LBNP, flight and centrifuge load. In: *Proc European Medical & Biological Engineering Conference EMBEC '99.* Vienna, Austria; 1999. pp. 1/458–459.
31. Hinghofer-Szalkay HG, König EM, Sauseng-Fellegger G, Zambo-Polz C. Biphasic blood volume changes with lower body suction in humans. *Am J Physiol.* 1992; 263(4 Pt 2):H1270-5.
32. van Hoeyweghen R, Hanson J, Stewart MJ, Dethune L, Davies I, Little RA, et al. Cardiovascular response to graded lower body negative pressure in young and elderly man. *Exp Physiol.* 2001; 86(3):427–35.
33. Hoppe M, Oskina D, Schmidt A, Kosch T. Odin's Helmet: A Head-Worn Haptic Feedback Device to Simulate G-Forces on the Human Body in Virtual Reality. In: *Proceedings of the ACM on Human-Computer Interaction.* New York, NY, USA: Association for Computing Machinery, Inc; 2021. pp. 1–15.
34. Johnson RL, Nicogossian AE, Bergman SA, Hoffler GW. Lower body negative pressure: the second manned Skylab mission. *Aviat Space Environ Med.* 1976; 47(4):347–53.
35. Kimmerly DS, O'Leary DD, Menon R, Gati JS, Shoemaker JK. Cortical regions associated with autonomic cardiovascular regulation during lower body negative pressure in humans. *J Physiol.* 2005; 569(Pt 1):331–45.
36. Krug E, Berg L, Lee C, Hudson D, Birke-Sorensen H, Depoorter M, et al. Evidence-based recommendations for the use of Negative Pressure Wound Therapy in traumatic wounds and reconstructive surgery: steps towards an international consensus. *Injury.* 2011; 42 Suppl 1:S1-12.
37. László Z, Rössler A, Hinghofer-Szalkay HG. Cardiovascular changes during and after different LBNP levels in men. *Aviat Space Environ Med. United States;* 1998; 69(1):32–9.
38. Lategola MT, Trent CC. Lower body negative pressure box for +Gz simulation in the upright seated position. *Aviat Sp Environ Med.* 1979; 50(11):1182–4.

39. Lathers CM, Charles JB. Use of lower body negative pressure to counter symptoms of orthostatic intolerance in patients, bed rest subjects, and astronauts. *J Clin Pharmacol.* 1993; 33(11):1071–85.
40. Lewkowicz R. Metoda oceny jakości odwzorowania przyspieszeń w symulatorach lotu. [Warszawa]: Lewkowicz; 2017.
41. Lewkowicz R, Kowaleczko G. Ocena jakości odwzorowania przyspieszeń w wirówce przeciążeniowej. In: Sibiński K, editor. *Mechanika w lotnictwie ML-XVIII.* Kazimierz Dolny: Polskie Towarzystwo Mechaniki Teoretycznej i Stosowanej; 2018. pp. 67–78.
42. Lewkowicz R, Krej M, Baran P, Dereń M, Dziuda Ł. Review of Lower Body Negative Pressure Applications To Simulate +Gz-Induced Cardiovascular Strain: Research History. *Polish J Aviat Med Bioeng Psychol.* 2023; 29(1):35–45.
43. Lindberg EF, Sutterer WF, Marshall HW, Headley RW, Wood EH. Measurement of cardiac output during headward acceleration using the dye-dilution technique. *Aerosp Med.* 1960; 31:817–34.
44. Lindenberger M, Olsen H, Länne T. Lower capacitance response and capillary fluid absorption in women to defend central blood volume in response to acute hypovolemic circulatory stress. *Am J Physiol Heart Circ Physiol.* 2008; 295(2):H867–73.
45. van Loon LM, Steins A, Schulte KM, Gruen R, Tucker EM. Computational modeling of orthostatic intolerance for travel to Mars. *npj Microgravity.* 2022; 8(1):20–2.
46. Lucertini M, De Angelis C, Martelli M, Zolesi V, Tomao E. Subjective visual vertical in erect/supine subjects and under microgravity: effects of lower body negative pressure. *Eur Arch Otorhinolaryngol.* 2011; 268(7):1067–75.
47. Ludwig DA, Krock LP, Doerr DA, Convertino VA. Mediating effect of onset rate on the relationship between +Gz and LBNP tolerance and cardiovascular reflexes. *Aviat Sp Environ Med.* 1998; 69(7):630–8.
48. Ly V, Velichala SR, Hargens AR. Cardiovascular, Lymphatic, and Ocular Health in Space. *Life.* 2022; 12(2):268.
49. Masica RM. A study to evaluate the suitability of a centrifuge as a dynamic flight simulator for F/A-18 strike fighter mission training. MSc. thesis. University of Tennessee; 2009.
50. Mikuliszyn R, Żebrowski M, Artur D, Różanowski K. LBNP as useful tool for pilot candidates selection to the Polish Air Force: A preliminary study. *J gravitational Physiol A J Int Soc Gravitational Physiol.* 2001; 8(1):P147-8.
51. Modak S, Singh AK, Gomez G. Human centrifuge: A tool for research and training. *Indian J Aerosp Med.* 2001; 45(2):101–5.
52. Musgrave FS, Zechman FW, Mains RC. Comparison of the effects of 70 degrees tilt and several levels of lower body negative pressure on heart rate and blood pressure in man. *Aerosp Med.* 1971; 42(10):1065–69.
53. Musgrave FS, Zechman FW, Mains RC. Changes in total leg volume during lower body negative pressure. *Aerosp Med.* 1969 Jun; 40(6):602–6.
54. Panton LB, Franke WD, Bleil DA, Baier SM, King DS. Effects of resistance training on cardiovascular responses to lower body negative pressure in the elderly. *Clin Physiol.* 2001; 21(5):605–11.
55. Polese A, Sandler H, Montgomery LD. Hemodynamic responses to seated and supine lower body negative pressure: Comparison with +Gz acceleration. *Aviat Sp Environ Med.* 1992; 63(6):467–75.
56. Repperger DW. A study of supermaneuverable flight trajectories through motion field simulation of a centrifuge simulator. *J Dyn Syst Meas Control.* 1992; 114:270–7.
57. Repperger DW, McCloskey K, Frazier J, Esken R, Roark M. Methodology for motion base simulation of closed loop supermaneuvers on a centrifuge simulator. In: *Aerospace and Electronics Conference, 1991 NAECON 1991, Proceedings of the IEEE 1991 National.* IEEE; 1991. pp. 849–55.
58. Schmedtje JF, Gutkowska J, Taylor AA. Reciprocity of hemodynamic changes during lower body negative and positive pressure. *Aviat Space Environ Med.* 1995; 66(4):346–52.
59. Schneider SM, Watenpaugh DE, Lee SMC, Ertl AC, Jon Williams W, Ballard RE, et al. Lower-body negative-pressure exercise and bed-rest-mediated orthostatic intolerance. *Med Sci Sports Exerc.* 2002; 34(9):1446–53.
60. Simonson SR, Norsk P, Greenleaf JE. Heart rate and blood pressure during initial LBNP do not discriminate higher and lower orthostatic tolerant men. *Clin Auton Res Off J Clin Auton Res Soc.* 2003; 13(6):422–6.
61. Śmietanowski M, Cudnoch-Jędrzejewska A, Dziuda Ł. Zastosowanie testu pionizacyjnego i podciśnienia wokół dolnej połowy ciała w badaniach odruchowej regulacji krążenia u ludzi. *Folia Cardiol.* 2015; 10(4):283–7.
62. Smith JJ, Porth CM, Erickson M. Hemodynamic response to the upright posture. *J Clin Pharmacol.* 1994; 34(5):375–86.
63. Smith ML, Raven PB. Cardiovascular responses to lower body negative pressure in endurance and static exercise-trained men. *Med Sci Sports Exerc.* 1986; 18(5):545–50.
64. Tomaselli CM, Frey MA, Kenney RA, Hoffler GW. Hysteresis in response to descending and ascending lower-body negative pressure. *J Appl Physiol (Bethesda, Md 1985).* 1987; 63(2):719–25.
65. Truszczyński O, Kowalczyk K. The polish centrifuge as a dynamic flight simulator. New application and ideas. *Polish J Aviat Med Psychol.* 2012; 18(3):71–80.

66. Turski BK. Use of LBNP Model for Assessment of Human Adaptation Mechanisms with Regard to +Gz Tolerance. *Polish J Aviat Med Psychol.* 2013; 19(1):49–54.
67. Turski BK, Gembicka-Kuzak DM, Dębiński W. Compensatory reactions during lower body negative pressure (LBNP) exposure, head-up tilt (HUT) and +Gz tolerance. *J gravitational Physiol.* 1996; 3(2):97–8.
68. Turski BK, Kuzak W, Debinski WB, Gembicka-Kuzak DM, Dabrowski OB. Application of multivariate statistical analysis to estimate +Gz tolerance based on the changes of hemodynamic parameters during lower body negative pressure (LBNP). *J Gravit Physiol.* 1995; 2(1).
69. Turski BK, Gembicka-Kuzak DM, Debinski WB, Kuzak W. Relationship between atrial natriuretic peptide (ANP), renin (PRA), aldosterone (PAC), hemodynamic responses to lower body negative pressure (LBNP) and +Gz tolerance. *J gravitational Physiol a J Int Soc Gravitational Physiol.* 1995; 2(1):P37-8.
70. Verghese CA, Prasad AS. Lower body negative pressure system for simulation of +Gz-induced physiological strain. *Aviat Space Environ Med.* 1993; 64(2):165–9.
71. Wang X. LBNP test as an estimation of G-tolerance (abstract). *Aviat Sp Environ Med.* 1989; 60(503).
72. Watenpaugh DE, Breit GA, Buckley TM, Ballard RE, Murthy G, Hargens AR. Human cutaneous vascular responses to whole-body tilting, Gz centrifugation, and LBNP. *J Appl Physiol (Bethesda, Md 1985).* 2004; 96(6):2153–60.
73. Whinnery JE, Gillingham KK. Medical standards for experimental human use in acceleration stress research. *Aviat Space Environ Med.* 1983; 54(3):241–5.
74. Wojtkowiak M. Badanie tolerancji ustroju na działanie przyspieszeń na podstawie oceny prędkości przepływu krwi w tętnicy skroniowej i zaburzeń wzrokowych. Warszawa: Wojskowy Instytut Medycyny Lotniczej; 1982. P. 147
75. Wolthuis RA, Bergman SA, Nicogossian AE. Physiological effects of locally applied reduced pressure in man. *Physiol Rev.* 1974; 54(3):566–95.
76. Zuzewicz K, Kempa G, Biernat B, Kwarecki K. Heart rate variability during centrifuge (+Gz) and lower body negative pressure (LBNP) in pilot candidates. *J gravitational Physiol A J Int Soc Gravitational Physiol.* 1996; 3(2):101–2.
77. g-Cueing Technology - Cranfield Simulation Retrieved 8 April 2024 from: <https://www.cranfieldsimulation.com/g-cueing-technology/>
78. G-Seats. Retrieved 8 April 2024 from: <https://www.moog.com/products/g-seats.html>
79. GS-5 G-Seat | SimXperience® Full Motion Racing Simulator Technologies. Retrieved 8 April 2024 from: <https://www.simxperience.com/shop/sx-gs5-001-gs-5-g-seat-711#attr=>